

# Evaluation of the protective layer formation of Ophthalmic Viscosurgical Devices in ex vivo porcine eyes using intraoperative Optical Coherence Tomography

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### Purpose



> We quantitatively determined thickness maps and applied segmentation

- > During cataract surgery the lens gets destroyed with ultrasound.
  - $\succ$  Fragments can potentially become projectiles that cause irreversible damage to the corneal endothelium.
- > To coat the endothelium with a protection layer, Ophthalmic Viscosurgical Devices (OVDs) are injected into the anterior chamber.
- > The protective properties and thickness of OVDs have previously been the subject of investigation, using fluorescein and a Scheimpflug camera [1, 2].
- > Protective properties are however still poorly understood.
- > We present a method to quantitatively evaluate the distribution of OVDs, using Optical Coherence Tomography (OCT) and a Convolutional Neural Network (CNN) in an ex vivo porcine eye model.

# Methods

- > We simulated cataract surgery (irrigation & aspiration (I/A) and phacoemulsification (phaco)) and used BSS-milk-solution (100:1) to generate contrast.
- > We imaged 10 different OVDs each 10 times
  - > Twice: each after I/A and after phaco.
- > Scan size 2.9 (Z) x 6 (X) x 6 (Y) mm<sup>3</sup>, sampled @ 1024 x 512 x 128 pixels. ➢ with ZEISS LUMERA® 700 with ZEISS RESCAN® 700. > Segmentation pipeline consists of > Manual segmentation path: we manually segmented ~3000 B-scans for training of the network. We segmented entire volumes to include all cases, inclusing artifacts like reflexes and air bubbles. Segmentation path (based on Unet [3]): automatically segmented >25k B-scans. > Our CNN is capable of segmenting 3 semantic categories: the cornea (Fig. 1: white), Background (fig. 1: black) and BSS-milksolution (Fig. 1: grey).

- to volumes (Fig. 2(1) A-F).
- > Maps revealed huge fluctuations of the individual measurements (Fig. 2(2) A-F).



Figure 2: (1) 3D-rendering of segmented and noise reduced OCT scan for better spatial understanding. (2) Example thickness maps after segmentartion. White arrows indicate air bubbles in the OVD layer.

- $\blacktriangleright$  Median thickness values ranged from 39 ± 599 µm (PROVISC®) up to  $1437 \pm 489 \,\mu m$  (Healon EndoCoat).
- > Cohesive OVDs have the thinnest layer values, followed by combisystems. Dispersive OVDs had the highest group median thickness value (Fig. 3).





**Figure 3:** Thickness value distribution of all OVDs as violin plots. Colored boxes *highlight different groups (from [4] – modified).* 

## Conclusion

- $\succ$  We measured for the first time the thickness of the OVD over a large FOV of 6 x 6 mm<sup>2</sup>.
- > We evaluated thickness layers of 10 different OVDs and acquired a data base of 200 OCT volumes from 100 porcine eyes.
- > Understanding layer formation and persistence over a large FOV

Input B-scan

Segmented mask

**Figure 1:** Architecture of the CNN for B-scan segmentation (modified U-Net).

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are essential steps for the comprehension of the protective properties of OVDs and potentially for

- $\succ$  Confirmation for surgeons that protection was during surgery.
- $\succ$  OVD manufacturers to improve the properties of their products.
- $\succ$  Our pipeline can be expanded for 3D-sementation which would increase the spatial accuracy of the segmentation.

#### References

[1] Yoshino M, Bissen-Miyajima H, Ohki S (2009). Jpn J Ophthalmol 53(1):62–64. doi:10.1007/s10384-008-0601-3

[2] Mori H, Yamada H, Toyama K, Takahashi K (2018). Heliyon 4(9):e00822. doi:10.1016/j.heliyon.2018.e00822

[3] O. Ronneberger et al., 2016, <u>https://doi.org/10.1007/978-3-319-24574-4\_28</u>

[4] M. Wuest & P. Matten et al., Translational Vision Science & Technology February 2022, Vol.11, 28. doi:<u>https://doi.org/10.1167/tvst.11.2.28</u>